

# UPCommons

## Portal del coneixement obert de la UPC

<http://upcommons.upc.edu/e-prints>

This is the Accepted Manuscript version of the work. The definitive Version of Record was published in *Zeitschrift für Naturforschung C*, <http://dx.doi.org/10.1515/znc-2021-0274>.

Hoyo, J.; Bassegoda, A.; Tzanov, T. Electrochemical quantification of biomarker myeloperoxidase. "Zeitschrift für Naturforschung. Section C, a journal of biosciences", 22 Febrer 2022. DOI [10.1515/znc-2021-0274](https://doi.org/10.1515/znc-2021-0274)

---

URL d'aquest document a UPCommons E-prints:

<https://upcommons.upc.edu/handle/2117/363520>

---

1                   **Electrochemical quantification of biomarker myeloperoxidase**

2

3                   Javier Hoyo<sup>1,2</sup>, Arnau Bassegoda<sup>1</sup>, Tzanko Tzanov<sup>1,\*</sup>

4    1) Grup de Biotecnologia Molecular i Industrial, Department of Chemical Engineering,

5    Universitat Politècnica de Catalunya, Rambla Sant Nebridi 22, 08222, Terrasa, Spain

6    2) Department of Physical-Chemistry, Universitat de Barcelona, 08028 Barcelona,

7    Spain.

8

9    \*Corresponding author: Dr. Tzanko Tzanov, tel.: +34 93 739 85 70, fax: +34 93 739 82

10   25, e-mail: [tzanko.tzanov@upc.edu](mailto:tzanko.tzanov@upc.edu)

11

12   **Keywords:**

13   myeloperoxidase, ABTS, electrochemical detection, disease biomarker

14

15

16 **Abstract**

17

18 Point of care testing (PoCT) devices permit precise and rapid detection of disease-related  
19 biomarkers contributing to an early disease diagnosis and administration of an appropriate  
20 treatment. The enzyme myeloperoxidase (MPO) is a relevant biomarker for infection and  
21 inflammation events assessment, however its direct electrochemical quantification is  
22 hindered by the limited accessibility to the iron atom in its active center. Herein, such  
23 hindrance of the MPO biomolecule is overcome using the redox mediator 2,2'-azino-  
24 bis(3-ethylbenzothiazoline-6-sulphonic acid) (ABTS). The charge involved in the  
25 electrochemical reduction of the MPO-oxidized ABTS is correlated with the  
26 concentration of MPO. The use of ABTS allowed for the electrochemical assessment of  
27 a wide range of MPO concentrations (10-1000 nM) including those reported for wound  
28 infections, chronic obstructive pulmonary disease and early adverse cardiac events. The  
29 developed electroanalytical approach is rapid and inexpensive, and thus suitable for  
30 implementation in PoCT devices.

31

## 32 **1. Introduction**

33 Early diagnosis of infections or internal injuries are key for an accurate treatment.[1]  
34 However, conventional diagnostic protocols are time consuming and require trained  
35 personnel to use complex instruments. The development of analytical methods for  
36 disease-related biomarkers implementable into point of care testing (PoCT) devices will  
37 contribute to cost-effective, precise and rapid diagnosis and appropriate treatment.  
38 Moreover, it will facilitate the implementation of affordable screening programs among  
39 the population with a high risk for developing these diseases.

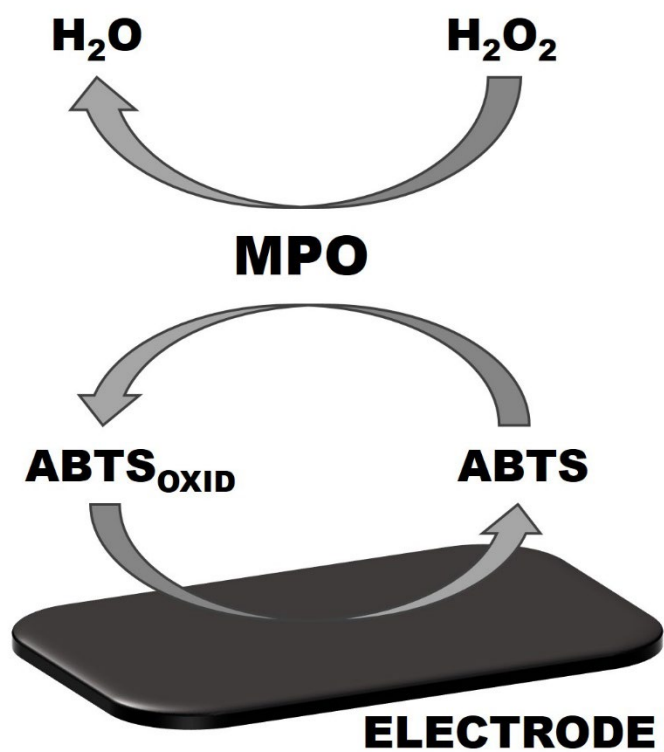
40 Myeloperoxidase (MPO) is a heme peroxidase enzyme released by activated neutrophils  
41 that catalyzes the oxidation of chloride ions to hypochlorous acid (HClO) using hydrogen  
42 peroxide as co-substrate.[2] MPO have been detected in wounds (200 to 1100 nM)[3]  
43 with bacterial infection, where HClO acts as a strong bactericidal agent, being specially  
44 abundant in non-healing chronic wounds with persistent bacterial colonization.[4,5] MPO  
45 has also been linked to other diseases related to inflammatory processes. Chronic  
46 obstructive pulmonary disease (COPD), characterized by chronic lung inflammation  
47 leading to progressive and irreversible airflow obstruction with periodic acute episodes  
48 of worsening exacerbations, can be early diagnosed by the presence in sputum of MPO  
49 (115-772 nM), interleukin-8 and leukotriene B<sub>4</sub>. [6] MPO is also overproduced in case of  
50 eroded arterial lesions due to neutrophil infiltration and activation into the inflamed and  
51 fissured blood vessels[7] thus, high levels of MPO in plasma (20-40 nM) are indicative  
52 of adverse cardiac events in patients with chest pain.[8] Consequently, MPO has been  
53 established as a relevant biomarker for assessment of infection, COPD and early adverse  
54 cardiac events. The rapid detection of MPO in body fluids will result in a drastic reduction  
55 of the morbidity and mortality caused by the abovementioned diseases and the related  
56 healthcare and economic burden.[9]

57 An ideal PoCT should be low-cost and easily operated such as an electrochemical readout  
58 system.[10] Electrochemical detection approaches are an attractive technology for  
59 microfluidic devices due to their inherent small size, low cost, high sensitivity, and  
60 portability for on-site analysis. Electrochemistry is a versatile and fast technique that has  
61 been widely used for a variety of applications such as permeability of membranes,[11,12]  
62 presence of metals in nanoparticles[13,14] and synthesis of metal nanoparticles.[15,16]  
63 In particular, electrochemistry has been successfully used for biomolecules, to assess their  
64 position in membranes,[17,18] quantify their presence in body fluids[19,20] and  
65 determine enzyme redox potentials.[21,22] PoCT devices based on electrochemistry of  
66 biomolecules have been presented for several purposes such as a non-invasive glucose  
67 level detector,[23] protein[24] and uric acid[25] detection. PoCT devices have also been  
68 developed for the MPO detection, but the tedious sample and electrode preparation, and  
69 the use of complex protocols requiring incubation with magnetic beads[26] and  
70 antibodies[27] limit their use.

71 The direct electrochemistry of MPO in solution is hindered due to the difficult access of  
72 the electrons from and to the heme group iron atom placed at the bottom of a deep crevice  
73 of the MPO structure.[28] Therefore, we propose the use of a redox mediator to facilitate  
74 the electron transfer, as has been previously reported for polymerization processes using  
75 other enzymes such horseradish peroxidases[29] or lignin oxidases (laccases).[30] In this  
76 context, we selected the mediator 2,2'-azino-bis(3-ethylbenzothiazoline-6-sulphonic  
77 acid) (ABTS) for the electrochemical detection of MPO. Our approach consists in the  
78 electrochemical reduction of the MPO-oxidized ABTS generating a measurable current  
79 (Fig 1) correlated to the MPO concentration in the sample. The current work establishes  
80 an electroanalytical approach based on the use of ABTS to quantify the presence of MPO

81 in liquid samples, which due to its simplicity, low cost and minimal set up requirements  
82 could be easily implemented in PoCT devices.

83



84

85

86 **Figure 1.** Scheme of the electrochemical quantification of MPO using redox mediator  
87 ABTS

88

89

90

## 91 **2. Materials and Methods**

### 92 2.1. Materials

93 Human myeloperoxidase (MPO) > 98 % purity was purchased from Planta Natural  
94 Products (ref: 700-03-001) as lyophilized powder, ABTS (98 %) and hydrogen peroxide  
95 were purchased from Sigma-Aldrich, and phosphate buffer saline (PBS) tablets were  
96 purchased from Fischer scientific. Disposable screen-printed gold electrodes (ref: DRP-  
97 C220AT) were purchased from Metrohm DropSens having working and auxiliary gold  
98 electrodes and a silver reference electrode and water was ultrapure MilliQ® (18.2  
99 MΩ·cm).

100

### 101 2.2. Electrochemical cell

102 The screen-printed electrodes were rinsed successively with ethanol and water prior  
103 drying with N<sub>2</sub> and placing in a home-made electrochemical cell of 200 μL that uses an  
104 o-ring to avoid liquid leakage. The electrochemical experiments were performed using a  
105 μAutolab Potentiostat (Ecochemie, NL) in a conventional three-electrode configuration.

106

### 107 2.3 Electrochemical experiments

108 Fresh ABTS solution was prepared dissolving the appropriate ABTS powder in PBS  
109 solution (pH 7.4) in milliQ grade water. Electrochemically oxidized (EC) ABTS stock  
110 solution was obtained by applying a constant potential (0.7 V) to fresh ABTS solution in  
111 the electrochemical cell until no color and current changes were registered. Fresh and EC-  
112 oxidized ABTS solutions at the desired concentrations were obtained by the appropriate  
113 dilution in PBS of the corresponding stock solutions. Lyophilized MPO was reconstituted  
114 in PBS and the appropriate amount of MPO stock was added to a PBS solution containing  
115 fresh ABTS (1 mM) and hydrogen peroxide (1 mM) to initiate an oxidation reaction  
116 incubated at room temperature (23 ± 1 °C) for 5 min to ensure the oxidation of ABTS by

117 the MPO. Cyclic voltammograms (CV) were performed at  $10 \text{ mV}\cdot\text{s}^{-1}$  and room  
118 temperature, scanning towards negative potentials. Chronoamperometric experiments  
119 were performed at 0.2 V and room temperature during 5 min.

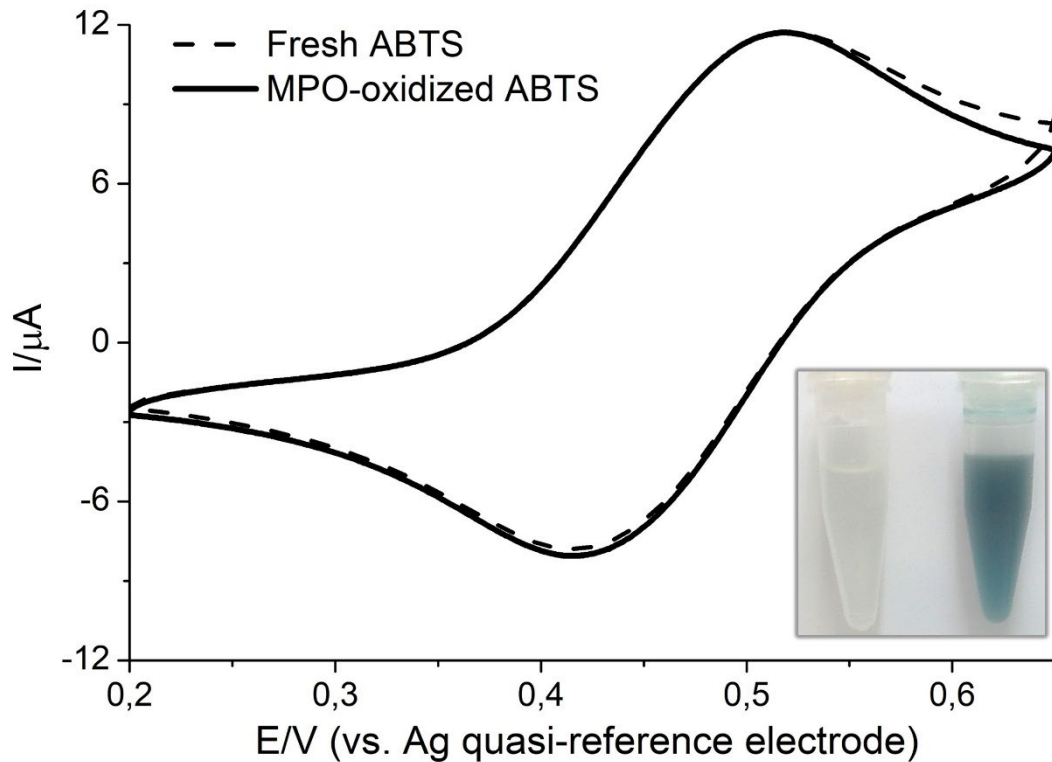
120

121



122 **Results and Discussion**

123 ABTS has been used as a substrate for MPO quantification in spectrophotometric  
124 techniques,[31] however, its suitability as a redox mediator for electrochemical  
125 quantification of MPO has not been demonstrated yet. The CV of ABTS (Fig 2) revealed  
126 a reversible redox behavior observing both the oxidation and reduction peaks without  
127 evidences of undesired reactions on the electrode surface. Therefore, the observed  
128 reversibility indicated the suitability of this molecule to be electrochemically detected  
129 after its oxidation by MPO.



130

131 **Fig 2.** Cyclic voltammograms of fresh ABTS and MPO-oxidized ABTS (MPO: 250nM,  
132 H<sub>2</sub>O<sub>2</sub>: 1mM, ABTS: 1mM). Inset: Fresh ABTS (left) and MPO-oxidized ABTS (right)  
133 solutions.

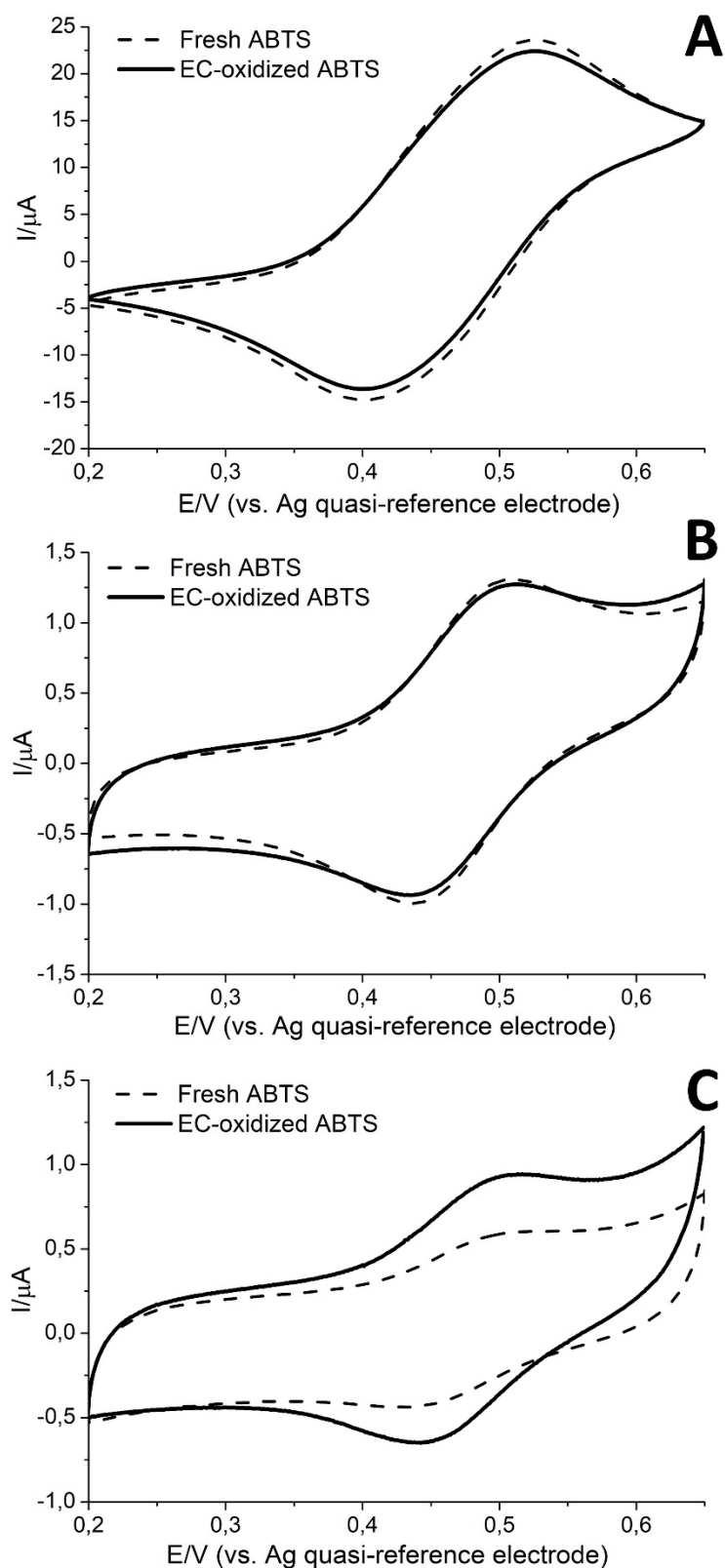
134

135 Despite MPO oxidizes ABTS, achieving the characteristic color change from transparent  
136 to intensive green[32] (Fig. 2), the differences in the cyclic voltammograms were not  
137 conclusive. The obtained electrochemical reduction scan produced a reduction current of  
138 equal magnitude than the control without enzyme. The presence of the reduction current  
139 peak may be related to the oxidation of ABTS during the electrochemical scan that starts  
140 in an oxidative potential. This process would occur at the surface of the electrode  
141 independently of the solution context, thus, obtaining similar electrochemical response  
142 for both fresh ABTS (control) and the sample with MPO-oxidized ABTS. To further  
143 confirm this phenomenon, dilutions from EC-oxidized ABTS stock and from fresh ABTS  
144 stock solutions were prepared and analyzed using cyclic voltammetry (Fig. 3). Similar  
145 CVs were obtained for both fresh ABTS and EC-oxidized ABTS at high concentrations  
146 (Fig. 3 A and B), while at low concentration, the EC-oxidized ABTS presented higher  
147 intensity current peaks than the fresh ABTS (Fig. 3C). This observation confirms that  
148 ABTS is electrochemically oxidized at high potentials during the reduction scan. The  
149 reduction current observed for ABTS has two contributions - from the initial EC-oxidized  
150 ABTS dilution and from the *in situ* ABTS oxidized during the reduction scan. Upon  
151 dilution of the ABTS samples, the contribution of the *in situ* ABTS oxidized is minor than  
152 the contribution from the initial EC-oxidized ABTS. A similar behavior is expected in  
153 case of using MPO to oxidize ABTS instead of EC. Therefore, cyclic voltammetry can  
154 only be applied to a low and narrow range of MPO concentrations and is not suitable for  
155 a PoCT electrochemical device.

156

157

158



159

160 **Fig 3:** Cyclic voltammograms of EC-oxidized and fresh ABTS solutions at several ABTS  
 161 concentrations: A) 500  $\mu\text{M}$ , B) 125  $\mu\text{M}$  and C) 25  $\mu\text{M}$

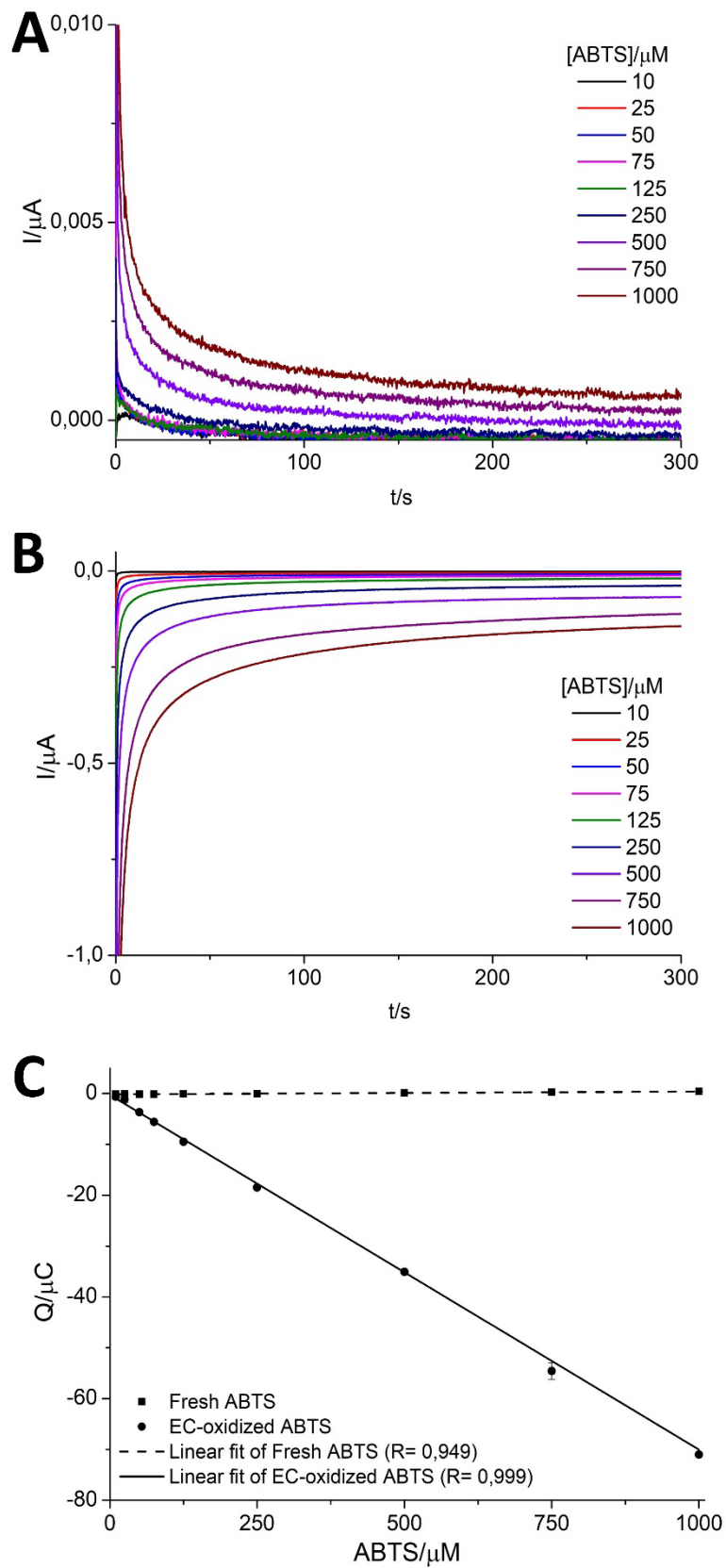
162 Alternatively, a chronoamperometric electrochemical method was employed, applying a  
163 constant reduction potential of 0.2V, according to the performed CVs (Fig. 3). This  
164 potential is out of the ABTS oxidation zone, thus decreasing the presence of EC-oxidized  
165 ABTS and its consequent contribution to the overall ABTS electrochemical reduction  
166 current. To assess the suitability of this method, the aforementioned reduction potential  
167 was applied to different dilutions of EC-oxidized ABTS and freshly prepared ABTS (Fig.  
168 4). The registered reduction currents analysis for both the fresh ABTS (Fig. 4A) and EC-  
169 oxidized ABTS (Fig. 4B) revealed a linear relationship according to the concentration of  
170 each redox specie (Fig. 4C). The large current difference between EC-oxidized ABTS  
171 and fresh ABTS coupled to the linear relationship indicate the suitability of the  
172 chronoamperometric method with the redox mediator ABTS for the electrochemical  
173 quantification of MPO.

174 To validate this method, freshly prepared ABTS was oxidized by MPO in concentrations  
175 found in exudates of infected wounds,[3] in blood from patients with coronary plaque  
176 erosion[8] and in sputum from patients with COPD.[6,33] The oxidation of fresh ABTS  
177 by different MPO concentrations resulted in green colored solutions electrochemically  
178 reduced at 0.2V (Fig 5A). Upon increasing the applied MPO concentration, a higher  
179 reduction charge was required to reduce the MPO-oxidized ABTS establishing a clear  
180 parabolic relationship (Fig. 5B). Therefore, the chronoamperometry of the redox mediator  
181 ABTS has been demonstrated as a promising electrochemical method for quantitative  
182 assessment of clinically relevant MPO concentration.

183 The simplicity and minimal electrode setup requirements of the developed approach pave  
184 the way for its implementation into PoCT devices for MPO detection. In these  
185 forthcoming sensors, the presented MPO electrochemical quantification can be combined  
186 with sample preparation steps according to the nature of the sample (blood, sputum,

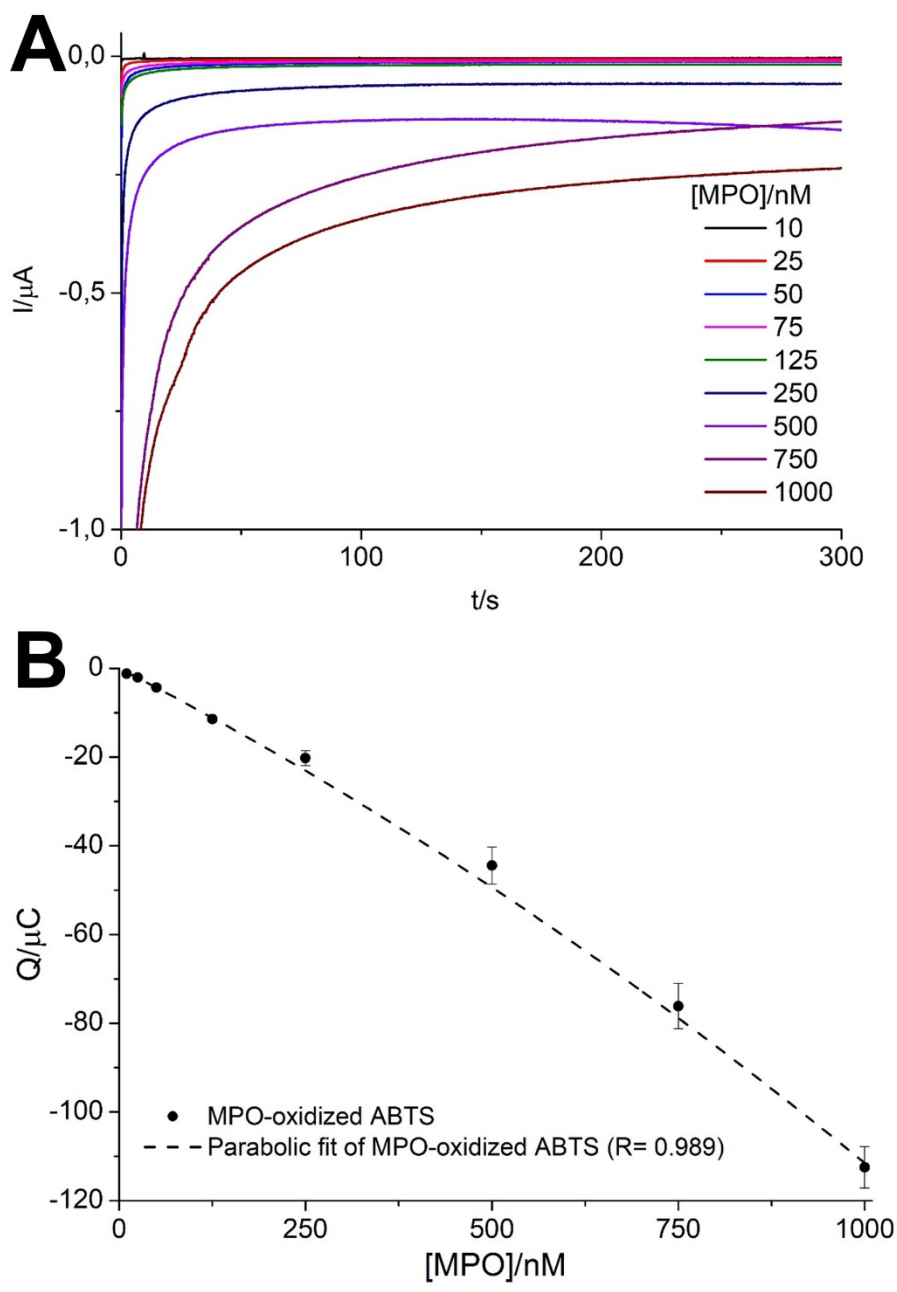
187 wound fluid) to avoid the risk of interfering substances. For instance, immunocapture  
188 with magnetic beads can separate MPO from other substances and concentrate it at the  
189 electrode surface[34] or paper-based microfluidics for sample fractionation.[35]

190



191

192 **Fig 4:** Chronoamperometry of A) fresh ABTS solutions, B) EC-oxidized ABTS and C)  
 193 reduction charge vs. ABTS concentration.



194

195 **Fig 5:** A) Chronoamperometry of ABTS oxidized (1 mM) by different MPO  
 196 concentrations in the presence of  $\text{H}_2\text{O}_2$  (1mM) and B) reduction charge vs. MPO  
 197 concentration.

198

199

200

201 **4. Conclusions**

202

203 The electrochemical reduction of the MPO-oxidized ABTS has been demonstrated as an  
204 analytical method to quantify the presence of MPO. ABTS has shown its capability to be  
205 used as a redox mediator for MPO, overcoming the access limitations to the MPO iron  
206 atom. Cyclic voltammetry was discarded as an electrochemical analytical method due to  
207 the high contribution of undesired processes to the peak intensity. Contrarily, the  
208 chronoamperometry technique at 0.2 V permitted the rapid (< 10 min) quantification of  
209 disease relevant MPO levels (10-1000 nM). Therefore, the developed simple and rapid  
210 electrochemical method represents a suitable analytical technique that could be  
211 implemented in PoCT devices for assessment of bacterial infection, COPD or adverse  
212 cardiac events.

213

214



215 **Acknowledgements**

216 This work was supported by the Spanish Ministry of Economy and Competitiveness,  
217 MINECO (Project PID2019-104111RB-I00).

218

219 **Notes**

220 The authors declare no conflicts of interest.

221

222 **Author Contributions**

223 The manuscript was written through contributions of all authors. All authors have given  
224 approval to the final version of the manuscript.

225

226 **Abbreviations**

227 2,2'-azino-bis(3-ethylbenzothiazoline-6-sulphonic acid) (ABTS), Chronic obstructive  
228 pulmonary disease (COPD), cyclic voltammogram (CV), electrochemically (EC),  
229 Myeloperoxidase (MPO), phosphate buffer saline (PBS), Point of care testing (PoCT)

230

231

232

233 **6. References**

- 234 [1] K. Ivanova, E. Ramon, J. Hoyo, T. Tzanov, Innovative Approaches for  
235 Controlling Clinically Relevant Biofilms: Current Trends and Future Prospects,  
236 *Curr. Top. Med. Chem.* 17 (2017) 1889–1914.  
237 <https://doi.org/10.2174/1568026617666170105143315>.
- 238 [2] M.B. Hampton, A.J. Kettle, C.C. Winterbourn, Inside the Neutrophil Phagosome:  
239 Oxidants, Myeloperoxidase, and Bacterial Killing, *J. Am. Soc. Hematol.* 92  
240 (1998) 3007–3017. <https://doi.org/10.1016/j.echo.2007.11.008>.
- 241 [3] A. Bassegoda, G. Ferreres, S. Pérez-Rafael, D. Hinojosa-Caballero, J. Torrent-  
242 Burgués, T. Tzanov, New myeloperoxidase detection system based on enzyme-  
243 catalysed oxidative synthesis of a dye for paper-based diagnostic devices,  
244 *Talanta.* 194 (2019) 469–474. <https://doi.org/10.1016/j.talanta.2018.10.065>.
- 245 [4] I. Stefanov, D. Hinojosa-Caballero, S. Maspoch, J. Hoyo, T. Tzanov, Enzymatic  
246 synthesis of a thiolated chitosan-based wound dressing crosslinked with chicoric  
247 acid, *J. Mater. Chem. B.* 6 (2018). <https://doi.org/10.1039/c8tb02483a>.
- 248 [5] A. Francesko, K. Ivanova, J. Hoyo, S. Pérez-Rafael, P. Petkova, M.M.  
249 Fernandes, T. Heinze, E. Mendoza, T. Tzanov, Bottom-up Layer-by-Layer  
250 Assembling of Antibacterial Freestanding Nanobiocomposite Films,  
251 *Biomacromolecules.* 19 (2018) 3628–3636.  
252 <https://doi.org/10.1021/acs.biomac.8b00626>.
- 253 [6] A. Zhu, D. Ge, J. Zhang, Y. Teng, C. Yuan, M. Huang, I.M. Adcock, P.J. Barnes,  
254 X. Yao, Sputum myeloperoxidase in chronic obstructive pulmonary disease, *Eur.*  
255 *J. Med. Res.* 19 (2014) 1–11. <https://doi.org/10.1186/2047-783X-19-12>.

- 256 [7] M.-L. Brennan, M.S. Penn, F. Ven Lente, V. Nambi, M.H. Shishehbor, R.J.  
257 Aviles, M. Goormastic, M.L. Pepoy, E.S. McErlean, E.J. Topol, S.E. Nissen, S.L.  
258 Hazen, Prognostic Value of Myeloperoxidase in Patients with Chest Pain, N.  
259 Engl. J. Med. 349 (2003) 1695–1702.
- 260 [8] G. Ferrante, M. Nakano, F. Prati, G. Niccoli, M.T. Mallus, V. Ramazzotti, R.A.  
261 Montone, F.D. Kolodgie, R. Virmani, F. Crea, High levels of systemic  
262 myeloperoxidase are associated with coronary plaque erosion in patients with  
263 acute coronary syndromes: A clinicopathological study, *Circulation*. 122 (2010)  
264 2505–2513. <https://doi.org/10.1161/CIRCULATIONAHA.110.955302>.
- 265 [9] J. Vestbo, S.S. Hurd, A.G. Agustí, P.W. Jones, C. Vogelmeier, A. Anzueto, P.J.  
266 Barnes, L.M. Fabbri, F.J. Martinez, M. Nishimura, R.A. Stockley, D.D. Sin, R.  
267 Rodriguez-Roisin, Global strategy for the diagnosis, management, and prevention  
268 of chronic obstructive pulmonary disease GOLD executive summary, *Am. J.*  
269 *Respir. Crit. Care Med.* 187 (2013) 347–365.  
270 <https://doi.org/10.1164/rccm.201204-0596PP>.
- 271 [10] Z. Nie, F. Deiss, X. Liu, O. Akbulut, G.M. Whitesides, Integration of paper-  
272 based microfluidic devices with commercial electrochemical readers, *Lab Chip*.  
273 10 (2010) 3163–3169. <https://doi.org/10.1039/c0lc00237b>.
- 274 [11] J. Hoyo, E. Guaus, J. Torrent-Burgués, Monogalactosyldiacylglycerol and  
275 digalactosyldiacylglycerol role, physical states, applications and biomimetic  
276 monolayer films, *Eur. Phys. J. E.* 39 (2016) 1–11.  
277 <https://doi.org/10.1140/epje/i2016-16039-0>.
- 278 [12] L. Zhao, X. Li, Y. Lin, L. Yang, P. Yu, L. Mao, Electrochemical impedance  
279 spectroscopic measurements of FCCP-induced change in membrane permeability

- 280 of MDCK cells, *Analyst*. 137 (2012) 2199–2204.  
281 <https://doi.org/10.1039/c2an35064e>.
- 282 [13] J. Hoyo, K. Ivanova, E. Guaus, T. Tzanov, Multifunctional ZnO NPs-chitosan-  
283 gallic acid hybrid nanocoating to overcome contact lenses associated conditions  
284 and discomfort, *J. Colloid Interface Sci.* 543 (2019) 114–121.  
285 <https://doi.org/10.1016/j.jcis.2019.02.043>.
- 286 [14] D. Martín-Yerga, Electrochemical detection and characterization of nanoparticles  
287 with printed devices, *Biosensors*. 9 (2019). <https://doi.org/10.3390/bios9020047>.
- 288 [15] P.M. Uberman, L.A. Pérez, S.E. Martín, G.I. Lacconi, Electrochemical synthesis  
289 of palladium nanoparticles in PVP solutions and their catalytic activity in Suzuki  
290 and Heck reactions in aqueous medium, *RSC Adv.* 4 (2014) 12330–12341.  
291 <https://doi.org/10.1039/c3ra47854h>.
- 292 [16] C. Zou, B. Yang, D. Bin, J. Wang, S. Li, P. Yang, C. Wang, Y. Shiraishi, Y. Du,  
293 Electrochemical synthesis of gold nanoparticles decorated flower-like graphene  
294 for high sensitivity detection of nitrite, *J. Colloid Interface Sci.* 488 (2017) 135–  
295 141. <https://doi.org/10.1016/j.jcis.2016.10.088>.
- 296 [17] J. Hoyo, E. Guaus, J. Torrent-Burgués, F. Sanz, Biomimetic monolayer films of  
297 digalactosyldiacylglycerol incorporating plastoquinone, *Biochim. Biophys. Acta*  
298 - *Biomembr.* 1848 (2015) 1341–1351.  
299 <https://doi.org/10.1016/j.bbamem.2015.03.003>.
- 300 [18] J. Hoyo, E. Guaus, J. Torrent-Burgués, F. Sanz, Electrochemical behaviour of  
301 mixed LB films of ubiquinone - DPPC, *J. Electroanal. Chem.* 669 (2012) 6–13.  
302 <https://doi.org/10.1016/j.jelechem.2012.01.020>.

- 303 [19] A.M. Attar, M.B. Richardson, G. Speciale, S. Majumdar, R.P. Dyer, E.C.  
304 Sanders, R.M. Penner, G.A. Weiss, Electrochemical Quantification of Glycated  
305 and Non-glycated Human Serum Albumin in Synthetic Urine, *ACS Appl. Mater.*  
306 *Interfaces*. 11 (2019) 4757–4765. <https://doi.org/10.1021/acscami.8b16071>.
- 307 [20] P. Giménez-Gómez, M. Gutiérrez-Capitán, F. Capdevila, A. Puig-Pujol, C.  
308 Fernández-Sánchez, C. Jiménez-Jorquera, Monitoring of malolactic fermentation  
309 in wine using an electrochemical bienzymatic biosensor for l-lactate with long  
310 term stability, *Anal. Chim. Acta*. 905 (2016) 126–133.  
311 <https://doi.org/10.1016/j.aca.2015.11.032>.
- 312 [21] V. Braunschmid, S. Fuerst, V. Perz, S. Zitzenbacher, J. Hoyo, C. Fernandez-  
313 sanchez, T. Tzanov, G. Steinkellner, K. Gruber, G.S. Nyanhongo, D. Ribitsch,  
314 G.M. Guebitz, A Fungal Ascorbate Oxidase with Unexpected Laccase Activity,  
315 *Int. J. Mol. Sci.* 21 (2020) 1–14. <https://doi.org/doi:10.3390/ijms21165754>.
- 316 [22] Y. Li, J. Zhang, X. Huang, T. Wang, Construction and direct electrochemistry of  
317 orientation controlled laccase electrode, *Biochem. Biophys. Res. Commun.* 446  
318 (2014) 201–205. <https://doi.org/10.1016/j.bbrc.2014.02.084>.
- 319 [23] A.J. Bandodkar, W. Jia, C. Yardimci, X. Wang, J. Ramirez, J. Wang, Tattoo-  
320 based noninvasive glucose monitoring: A proof-of-concept study, *Anal. Chem.*  
321 87 (2015) 394–398. <https://doi.org/10.1021/ac504300n>.
- 322 [24] D. Zhang, Y. Lu, Q. Zhang, L. Liu, S. Li, Y. Yao, J. Jiang, G.L. Liu, Q. Liu,  
323 Protein detecting with smartphone-controlled electrochemical impedance  
324 spectroscopy for point-of-care applications, *Sensors Actuators, B Chem.* 222  
325 (2016) 994–1002. <https://doi.org/10.1016/j.snb.2015.09.041>.
- 326 [25] J. Guo, Uric acid monitoring with a smartphone as the electrochemical analyzer,

327 Anal. Chem. 88 (2016) 11986–11989.  
328 <https://doi.org/10.1021/acs.analchem.6b04345>.

329 [26] J. Moral-Vico, J. Barallat, L. Abad, R. Olivé-Monllau, F.X. Muñoz-Pascual, A.  
330 Galán Ortega, F.J. del Campo, E. Baldrich, Dual chronoamperometric detection  
331 of enzymatic biomarkers using magnetic beads and a low-cost flow cell, *Biosens.*  
332 *Bioelectron.* 69 (2015) 328–336. <https://doi.org/10.1016/j.bios.2015.02.042>.

333 [27] K.C. Lin, V. Kunduru, M. Bothara, K. Rege, S. Prasad, B.L. Ramakrishna,  
334 Biogenic nanoporous silica-based sensor for enhanced electrochemical detection  
335 of cardiovascular biomarkers proteins, *Biosens. Bioelectron.* 25 (2010) 2336–  
336 2342. <https://doi.org/10.1016/j.bios.2010.03.032>.

337 [28] M.J. Davies, Myeloperoxidase-derived oxidation: mechanisms of biological  
338 damage and its prevention, *J Clin Biochem Nutr.* 48 (2011) 8–9.  
339 <https://doi.org/10.3164/jcbrn.11>.

340 [29] K. Won, Y.H. Kim, E.S. An, Y.S. Lee, B.K. Song, Horseradish peroxidase-  
341 catalyzed polymerization of cardanol in the presence of redox mediators,  
342 *Biomacromolecules.* 5 (2004) 1–4. <https://doi.org/10.1021/bm034325u>.

343 [30] R. Bourbonnais, M.G. Paice, Oxidation of non-phenolic substrates, *FEBS Lett.*  
344 267 (1990) 99–102. [https://doi.org/10.1016/0014-5793\(90\)80298-w](https://doi.org/10.1016/0014-5793(90)80298-w).

345 [31] A. Hasmann, E. Wehrsuetz-Sigl, A. Marold, H. Wiesbauer, R. Schoeftner, U.  
346 Gewessler, A. Kandelbauer, D. Schiffer, K.P. Schneider, B. Binder, M. Schintler,  
347 G.M. Guebitz, Analysis of myeloperoxidase activity in wound fluids as a marker  
348 of infection, *Ann. Clin. Biochem.* 50 (2013) 245–254.  
349 <https://doi.org/10.1258/acb.2011.010249>.

- 350 [32] S.S. More, P.S. Renuka, K. Pruthvi, M. Swetha, S. Malini, S.M. Veena, Isolation,  
351 purification, and characterization of fungal laccase from *Pleurotus* sp., *Enzyme*  
352 *Res.* 2011 (2011) 1–8. <https://doi.org/10.4061/2011/248735>.
- 353 [33] E. Bathoorn, J.J.W. Liesker, D.S. Postma, G.H. Koëter, M. van der Toorn, S. van  
354 der Heide, H.A. Ross, A.J.M. van Oosterhout, H.A.M. Kerstjens, Change in  
355 inflammation in out-patient COPD patients from stable phase to a subsequent  
356 exacerbation, *Int. J. COPD.* 4 (2009) 101–109.  
357 <https://doi.org/10.2147/copd.s4854>.
- 358 [34] X. Zhang, Z. Wang, H. Xie, R. Sun, T. Cao, N. Paudyal, W. Fang, H. Song,  
359 Development of a magnetic nanoparticles-based screen-printed electrodes  
360 (MNPs-SPEs) biosensor for the quantification of ochratoxin A in cereal and feed  
361 samples, *Toxins (Basel).* 10 (2018). <https://doi.org/10.3390/toxins10080317>.
- 362 [35] J. Noiphung, T. Songjaroen, W. Dungchai, C.S. Henry, O. Chailapakul, W.  
363 Laiwattanapaisal, Electrochemical detection of glucose from whole blood using  
364 paper-based microfluidic devices, *Anal. Chim. Acta.* 788 (2013) 39–45.  
365 <https://doi.org/10.1016/j.aca.2013.06.021>.
- 366